

“SUPER-SHOES” IN DISTANCE RUNNING: IS THERE A POSSIBLE DOWNSIDE IN TRAINED WOMEN?

Max R. Paquette¹, Eddie Martinez¹

College of Health Sciences, University of Memphis¹

Although “super-shoes” provide a metabolic advantage, anecdotal suggest that consistent wear may contribute to development of knee and hip overuse injuries. The purpose of this study was to compare these injury-related running biomechanics variables between “super-shoes” and traditional training shoes in female distance runners. 18 competitive female runners ran for 5min on a treadmill at 3.6 m/s in “super-shoes” (SUPER) and control shoes (CON) while 3D kinematic and ground reaction force data were collected. Peak knee abduction moment and peak hip internal rotation and abduction moment were larger in SUPER compared to CON but no other biomechanical variables were different between shoes. Findings from this study suggest that “super-shoes” may increase knee loading compared to traditional shoes in female distance runners.

KEYWORDS: running, shoes, biomechanics, endurance, women

INTRODUCTION: The world-wide growth in running participation over the last decades has contributed greatly to both consumer and scientific interest in running shoes. Recently, marketing efforts from shoe companies and drastically improving endurance running performances have, arguably, made shoe technology one of the most debated topics in the running world. Advancing technology to improve various shoe characteristics has led to the widely used term, “super-shoes.” These shoes are defined as racing or competition shoes designed to improve endurance running performance by reducing the energetic costs or oxygen consumption at a given speed (i.e., running economy; RE). Although “super-shoes” provide a metabolic advantage over traditional footwear, anecdotal reports from elite-level athletes, coaches, and clinicians suggest that consistent wear in training may have contributed to incidences of knee and hip overuse injuries. To date, no studies have been conducted to quantify the magnitude of certain injury-related biomechanical variables between “super-shoes” and traditional training running shoes. For example, higher peak knee (Noehren et al., 2014) and hip adduction (Pohl et al., 2008), peak hip internal rotation (Noehren et al., 2007), peak knee abduction moment, knee abduction impulse (Stefanyshyn et al., 2006), and peak hip abduction moment (Eskofier et al., 2012) have been associated with various running-related injuries. The soft, although resilient, midsole foam of “super-shoes” may increase allow for more frontal and transverse plane motion (e.g., frontal plane rearfoot eversion, hip adduction, knee abduction) of the lower limb to possibly yield greater magnitudes of the aforementioned injury-related knee and hip biomechanical variables. The purpose of this study was to compare these injury-related running biomechanics variables between “super-shoes” and traditional training shoes in female distance runners. We hypothesized that “super-shoes” would produce greater magnitudes for some of these injury-related biomechanical variables compared to traditional training shoes.

METHODS: *Participants:* 18 competitive female runners of various foot strike patterns were recruited for this study. All participants had prior experience in “super-shoes” for competition (i.e., to reduce familiarization effects) and to be included, were required to have completed a half marathon in under 1h44min, a 10km in under 47min, or a 5km in under 22min in the 6 months prior to testing.

Procedures: An 8-camera three-dimensional (3D) motion capture system (240 Hz, Qualysis AB, Goteburg, Sweden) and an instrumented force treadmill (1200 Hz, Bertec, Columbus, OH,

USA) were used to simultaneously to collect kinematic and ground reaction force (GRF) data during running trials, respectively. In addition, a metabolic system (TrueOne 2400; ParvoMedics, Murray, Utah, USA) was used to collect expired gases. Participants performed a five-minute warm-up on the experimental treadmill at a self-selected speed in their own running shoes. Participants then completed the experimental testing protocol of 5 minute running bouts at a speed of 3.6 m/s (i.e., 7min30s per mile) on the force instrumented treadmill in two shoe conditions: 1) the “super-shoe” condition (Nike Vaporfly Next% 2TM; SUPER) and 2) the control shoe condition (Nike Pegasus 38TM; CON). The SUPER condition had a mass of 176 g, stack height of 32 mm in the forefoot and 40 mm in heel, and a heel-to-to offset of 8 mm. The CON condition had a mass of 248 g, stack height of 23 mm in the forefoot and 33 mm in heel, and a heel-to-to offset of 10 mm. A randomized and mirrored (e.g., ABBA) testing order was used for experimental trials (Hoogkamer et al., 2018). After reflective markers were placed on the participants, participants were fitted with a rubber facemask (covering the nose and mouth) connected to the metabolic system via a breathing tube. Participants then ran for five minutes (until physiological steady-state is reached [i.e., plateau in VO₂ with RER below 1.05]) on the instrumented treadmill at the testing speed in the first shoe condition. Participants received approximately 7-8 minutes of rest before the start of testing in the second shoe condition. Kinematic and GRF data were collected for 15 seconds in the last minute of the first trials in each shoe condition.

Data Analyses: Visual3D software (C-Motion, Germantown, MD, USA) was used to process and analyse kinematic and kinetic variables from the running trials. Kinematic data were interpolated using a least-squares fit of a 3rd order polynomial, with a three data point fitting and a maximum gap of 10 frames. Kinematic and GRF data were filtered using a low-pass Butterworth filter with cut-off frequencies of 8 Hz and 40 Hz, respectively. A right-hand rule with a Cardan rotational sequence (x-y-z) was used for the 3D angular computations where x represents the medial-lateral axis, y represents the anterior-posterior axis, and z represents the longitudinal axis. Newtonian inverse dynamics was used to calculate net internal joint moments normalized to body mass (Nm·kg⁻¹) during the stance phase.

Statistical Analyses: Paired sample t-tests (SPSS 24.0, IBM) were used to compare footwear conditions for all dependent variables. Cohen’s *d* effect sizes were calculated to assess the effect magnitudes between footwear conditions (i.e., small: $d \leq 0.2$, moderate: $0.2 < d < 0.8$; large: $d \geq 0.8$). The significance level was set at $p \leq 0.05$.

RESULTS: Peak knee abduction moment (~7.5%), peak hip internal rotation (~23%), and peak hip abduction moment (~6.5%) were moderately larger in SUPER compared to CON (Table 1; Figure 1). Peak knee abduction moment, peak hip internal rotation, and peak hip abduction moment in the SUPER (compared to CON) increased in 61%, 67%, and 60% of runners, respectively.

Table 1. Sagittal plane joint kinematics and kinetics in “super-shoe” (SUPER) and control (CON) conditions (mean ± SD).

Variables	SUPER	CON	p	<i>d</i>
Peak Eversion (deg)	18.5 ± 4.6	18.8 ± 5.0	0.38	0.06
Mean Frontal Knee (deg)	-0.5 ± 3.3	-0.3 ± 2.4	0.40	0.06
Mean Transverse Knee (deg)	-0.4 ± 4.6	-1.7 ± 3.6	0.07	0.32
Peak Knee Valgus (deg)	-3.8 ± 3.5	-3.6 ± 2.4	0.42	0.04
Peak Knee Abduction Moment (Nm/kg)	-1.63 ± 0.43	-1.51 ± 0.28	0.04	0.33
Knee Abduction Impulse (Nm·s/kg)	-0.16 ± 0.03	-0.16 ± 0.03	0.37	0.05
Peak Hip Internal Rotation (deg)	10.9 ± 4.1	8.9 ± 4.6	0.01	0.47
Peak Hip Adduction (deg)	10.0 ± 3.3	10.0 ± 3.1	0.47	0.01
Peak Hip Abduction Moment (Nm/kg)	-3.3 ± 0.4	-3.1 ± 0.3	0.02	0.53

and hip injuries from “super-shoe” wear. Future studies should more systematically study injury development in distance runners from controlled training exposures in different types of shoes including “super-shoes”.

REFERENCES

- Eskofier BM, Kraus M, Worobets JT, Stefanyshyn DJ, Nigg BM. Pattern classification of kinematic and kinetic running data to distinguish gender, shod/barefoot and injury groups with feature ranking. *Comput Methods Biomech Biomed Eng*. 2012;15(5):467–474. doi:10.1080/10255842.2010.542153
- Hoogkamer W, Kipp S, Frank JH, Farina EM, Luo G, Kram R. A Comparison of the Energetic Cost of Running in Marathon Racing Shoes. *Sports Medicine*. 2016;48(4):1009–19.
- Noehren B, Schmitz A, Hempel R, Westlake C, Black W. Assessment of strength, flexibility, and running mechanics in men with iliotibial band syndrome. *J Orthop Sports Phys Ther*. 2014;44(3):217–222. doi:10.2519/jospt.2014.4991
- Noehren B, Davis I, Hamill J. ASB clinical biomechanics award winner 2006 prospective study of the biomechanical factors associated with iliotibial band syndrome. *Clin Biomech (Bristol, Avon)*. 2007;22(9):951–956. doi:10.1016/j.clinbiomech.2007.07.001
- Pohl MB, Mullineaux DR, Milner CE, Hamill J, Davis IS. Biomechanical predictors of retrospective tibial stress fractures in runners. *J Biomech*. 2008;41(6):1160–1165. doi:10.1016/j.jbiomech.2008.02.001
- Stefanyshyn DJ, Stergiou P, Lun VM, Meeuwisse WH, Worobets JT. Knee angular impulse as a predictor of patellofemoral pain in runners. *Am J Sports Med*. 2006;34(11):1844–1851. doi:10.1177/0363546506288753

ACKNOWLEDGEMENTS: The authors would like to thank Nike, Inc for providing the footwear for this study.